

Dual Filter Based Images Fusion Algorithm for CT and MRI Medical images

P .Maadhurya¹, P.Tejasri², T.Keerthi³, M.Thabitha⁴

¹Maadhurya.penumtecha@gmail.com,²tejasribtech99@gmail.com,

³keerthitetalal1998@gmail.com, ⁴thabithamorathoti@gmail.com

ABSTRACT: In this our methodology depends on two filters the first is the laplacian filter and the subsequent one is the guided filter, here the laplacian filter is utilized for denoising the detailed coefficients and the subsequent filter guided filter is utilized for refinement of both approximation and detailed coefficients of computer tomography(CT) and magnetic resonance imaging(MRI). In this first both the input image were converted in to frequency domain by utilizing wavelet transform then we acquired approximation coefficient and detailed coefficient and another two coefficient of computer tomography(CT) and magnetic resonance imaging(MRI) . Images Presently two weight maps are acquired after the procedure of comparison. The comparison is done between the two approximation coefficients and two detailed coefficients and dependent on this coefficients guided filter is planned. Here guided filter will manage a image relating to the weighted maps and the weight maps are smoothed based on guided filter and this is mainly utilized as an information image. Subsequently the weighted fusion algorithm will fuse the both CT and MRI pictures. The full clear fused image is possibly acquired when the CT and MRI images are refined by inverse wavelet transform. From the above outcomes, it is very well may be seen that the proposed framework gives better outcomes when contrasted with existing framework. Just as the proposed framework will give maximum amount of contribution in detail way.

Keywords: Fusion, Guided Filter, Weighted Fusion, haar wavelet Transform, Laplacian Filter.

I.INTRODUCTION

Fundamentally clinical diagnosis utilizes two kinds of techniques.one is CT and another is MRI[1]. The principle goal of the CT is to examine the human body. The CT check gives differential outspread ingestion and densities relying upon the X-beams. X-beams comprises of delicate tissues and hard tissues . Hard tissues has high thickness of resolution and soft tissues has low thickness resolution.

CT gives the data about the lung analysis and interstitial lung diseases. For this CT filter utilizes high thickness of resolution. X-ray gives the data about the apprehensive system, muscle, feet by utilizing low thickness of resolution. The CT and MRI strategies are entirely unexpected to each other. For instance CT filtering utilizes both delicate and hard tissues and MRI utilizes just delicate tissues[2]. The CT and MRI strategies will intertwine the images of new patient. The fused image will gives the data about the size, location and state of the image. The main goal of using radiotherapist is to obtain the values of CT and MRI images and the values of fused image. By doing this we get more accuracy. This exactness will push the patient to accuracy the objective treatment. Here the host images are deteriorated by multi goals coefficient. These coefficients will pick the fusion calculation to get the resultant picture. The fusion calculation will give contribution about the commotion delicate and weighted normal fusion. This calculation will deliver the outcomes in simple manner. Fundamentally image fusion calculation is utilized in image preparing field. But in this different filter to be embraced for better performance. These filters will smooth the image just as edge extractions and image enhancement. After playing out

every one of these activities, linear shift invariant filter and shift invariant filter will be utilized. This process is like the median filter imaging. But here the above filters will not give the constant weight maps. The constant weight maps can be obtained using guided image. The process of obtaining fixed weight maps is called guided filter. The guided filter not just produce the contribution for the source image yet in addition gives the characteristics of the information image, The GF strategy comprises of qualities of edge. This GF strategy will beat the confinements and too as this calculation will create high effectiveness, utilizes little size and linearity. Essentially, invariant filters are utilized as Gaussian filters. These Gaussian filters are autonomous to convey the contribution from guided image. Here GF will decide the idea of guided image in successful manner. Here the fundamental reason for guided image is to smooth the edges. In the same way we accept the guided image as either input image or other image. In image improvement procedure the input image produces effective outcomes contrasted with others. So also, it produces noise reduction and image fusion by utilizing the Gaussian filter. A weighted image fusion utilizing CT and MRI clinical images is proposed in this paper. This framework will interweave the images adaptively and afterward Wavelet transform is used. Essentially one approximation coefficient, three wavelet coefficient of CT and MRI images are gained by utilizing wavelet transform on CT and MRI accommodating images autonomously. Two approximation coefficients are utilized to keep up the general state of source image. After two approximations, wavelet coefficients are used after de-noising with laplacian filter. These are analysed by pixel by pixel to get the weight maps. The weight maps are typically huge and edge obscuring. So as to acquire the fused image the weight maps filling in as the information and the differentiating farthest reaches of noteworthy worth and positive coefficient filling in as the guided image. GF is used to smooth the weight maps and refined weight maps are gotten, along these lines refined guide of each image is one of a kind and fixed out by the characteristics of the image to be intertwined with help of refined weight maps.

II.METHODOLOGY

Introduction to GF:

The guided filter processes the separating yield by considering the substance of a direction image, which can be simply the input image or another distinctive image. The guided filter can be utilized as an edge-saving smoothing administrator like the mainstream two-sided images, however it has better practices close to edges.

The yield image 'O' of GF is a linear transform of a guided image I in a window showed at pixel 'k' and the filter yield at pixel I is settled as looks for after

$$oi = akIi + bk \quad \forall, i \in wk \quad (1)$$

Where wk is the square window of clear 'r' from condition (1) we can see that

$\nabla O = a \nabla I$, where ∇O and ∇I are the tendency of yield image 'O' and guided image 'T', from this we can know 'O' has an edge just in the event that 'T' has an edge, and are straight coefficients in wk and can be reviewed by limiting the underneath cost work in adjoining window.

$$(a_k b_k) = \sum_{i \in wk} ((a_k I_i + b_k - P_i)^2 + \epsilon a_k^2) \quad (2)$$

Here ϵ is utilized to change the separating sway which is taken as huge parameter. Going to the parameter p_i , this is the input image an incentive at pixel I, finally least-square method is utilized to decide, a_k, b_k

$$a_k = (\frac{1}{|wk|} \sum_{i \in wk} I_i p_i - \mu_k \bar{p}_k) / (\sigma k^2 + \epsilon)$$

$$b_k = \bar{P}_k - a_k \mu_k \quad (3)$$

Where μ_k and σk^2 are mean and deviation estimations of the guided image in wk . $|wk|$ implies pixel number in wk , \bar{P}_k is mean estimation of input image in wk . For the estimations of straight coefficients of each pixel is depicted by different direct limits, and the estimation of oi is different when it is decided in different windows in order to handle this issue each possible regard of oi ought to be arrived at the midpoint of first

$$o_i = \frac{1}{|w|} \sum_{iWk} (a_k l_i + b_k) \\ = \bar{a}_i l_i + \bar{b}_i$$

Where $\bar{a}_i = \frac{1}{|w|} \sum_{iWk\epsilon} a_k$ and
 $\bar{b}_i = \frac{1}{|w|} \sum_{iWk\epsilon} b_k$

From the above conditions ∇O is the straight transform of ∇I in light of the fact that the immediate coefficients a_i , b_i transforms spatially. The coefficients are only yield of an average filter and their edge should be significantly more diminutive than that of I near the strong edges, when everything is said in done coefficients are in this manner still we have $\nabla O = \nabla I$.

That suggests clear edges in I can be generally kept up in ' O ' which connotes the edge protecting nature of the GF.

Determination of parameter of GF:

$G_{y,\epsilon}(P,I)$ is used to connote essentially the both info picture and guided picture are indicated independently right now. Next r and ϵ coefficients will decide the size of channel and just as it decide the GF separately.

In the above condition that $\epsilon=0$ unmistakably $a_k=1$, $b_k=0$ from the above conditions, when $O = I$ for this circumstance no sifting sway is accessible at the present time if $\epsilon>0$ let us think around two cases.

Case 1: "High changes", i.e. $\epsilon\sigma_k^2 >> \epsilon$, so $a_k=1$ and $b_k=0$ at that point the sifting effect of those qualities are very frail and it very well may be used keep up edges of picture.

Case 2: "Level fix", i.e. $\epsilon\sigma_k^2 << \epsilon$, (In wk , the estimation of guided picture is stays steady so $a_k=0$ and $b_k=\mu_k$. Thus the GF is known as weighted normal channel.

From the above assessment the parameter ϵ is the criteria to pick a high vacillation or level fix. The patches with a distinction fundamentally littler than ϵ are smooth and with a change more prominent than ϵ are made sure about under the condition that window size can't be changed i.e the more minute the ϵ the more obvious part of edge protecting, the more noteworthy ϵ the more clear filtering impact.

$\epsilon = \sigma^2 10^{-5}$ is considered right now on the reference, with the essential contribution of GF, the base estimations of 'r' is '1' and the best estimation of 'r' is (Min (width-1, stature 1))/2 where width is the pixel number of guided picture in X-bearing and tallness is the pixel number of guided picture in Y-course, Min is the action for least.

III.EXISTING ALGORITHMS

In this article the proposed algorithm is compared with the following three existing algorithms

Choose-max fusion algorithm:

Contrasting the black estimation of every pixel in the original image and consider the greater gray value an estimation of the combined image. The various strides in Choose-max combination computation is as follows

Step1: The CT image is decayed in to approximation coefficient A_1 and another three coefficient D_1 , V_1 , and H_1 by the using wavelet transform after the registration. And also MRI image is decayed in to approximation coefficient A_2 and another three coefficient D_2 , V_2 , and H_2 .

Step2: After the inspection of four arrangements of coefficients of the both input images the fused approximation and detailed coefficients A_C , H_C , V_C , D_C will be obtained based on the following formula

$$S1=s1, s1>=s2$$

$$S2, s2>=s1$$

Where $s1$ and $s2$ means approximation and detailed coefficients A_1 , A_2 , D_1 , D_2 , H_1 , H_2 and V_1 , V_2 S denotes the fused approximation and detailed coefficients of A_C , H_C and D_C , V_C

Step 3: The fused image is obtained by taking invert wavelet transform of the fused approximation and detailed coefficients A_C , H_C , V_C and D_C .

Intuitionistic fuzzy interference fusion algorithm:

It is a development related to the man-made thinking and in this technique the strategy for impedance is acquired by

duplicating the human thinking. This strategy comprehends the mapping among input and output.

The steps involved in fuzzy interface fusion algorithm is as follows

Step1: CT and MRI input image registration

Step2: By the use of wavelet transform CT image is disintegrated into estimation coefficient A1 and three quick and dirty coefficients H1, V1, D1. So furthermore MRI image is disintegrated into worth coefficient A2 and three wavelet coefficients H2, V2, D2.

Step 3: Worth and coefficients after the combination A1, H1, V1 and D1 can be acquired by intuitionistic fuzzy obstacle method separately .

Step 4: Fused image can be obtained after the use of reverse wavelet transform of intertwist unpleasant coefficients and three wavelet coefficients A1, H1, V1 and D1.

Gf based CT and MRI images fusion algorithm:

Step1: CT and MRI input registration

Step2: CT image is disintegrated into gathered coefficient A1 and three point by point coefficients H1,V1, and D1 by the usage of wavelet transform.in like way MRI image is disintegrated into gathered coefficient A2 and three quick and dirty coefficients H2,V2 and D2.

Step 3: by taking the pixel values of approximation coefficients of CT and MRI images the weight maps are acquired and these weight maps are filling in as information image and relating approximation coefficients filling in as the guided image for the guided filter.

$$W1=1, \text{ if } A1>A2$$

$$0, \text{ otherwise}$$

$$W2=1, \text{ if } A2>A1$$

$$0, \text{ otherwise}$$

Guided filter refine the weight maps and gives the new weight maps those are known as refined weight maps

$$M1=G^{\gamma,\varepsilon}(W1, A1)$$

$$M2=G^{\gamma,\varepsilon}(W2, A2)$$

Step 4: By the use of weighted fusion computation, the approximation and detailed coefficients can be acquired.

Step 5: Fusion image can be gotten by the utilization of opposite wavelet transform of the fused worth and coefficients.

IV. SCHEME OF PROPOSED ALGORITHM

After the selection of image wavelet transform is applied to CT and MRI images. So that the CT image is crumbled into four coefficients as A1, H1,V1 and D1.similarly MRI picture is broken down into A2,H2,V2 and D2. Here A1 and A2 coefficients contain the data about the limits of the input pictures and the rest of the coefficients H1, V1,D1 and H2,V2,D2 contain the data about the information inside the information image.

Here we will consider just the approximation and detailed coefficients in order to apply fusion algorithm since they contain the two information and commotion. Weight maps are acquired after the examination of pixel approximation coefficients and detailed coefficients. What's more, on the off chance that $A1 > A2$, $H1 > H2$, $V1 > V2$ and $D1 > D2$, at that point $W1 = 1$ otherwise 0 additionally in the event that $A2 > A1$, $H2 > H1$, $V2 > V1$ and $D2 > D1$, at that point $W2 = 1$ otherwise 0.

$$W1 = \max(A1, H1, V1, D1)$$

$$W2 = \max(A2, H2, V2, D2)$$

The weight maps got may contain edge obscure and some noise. So the weight maps will be given to the guided filter. The guided filter will smooth the weight maps lastly we will get the refined weight maps as M1 and M2.

$$M1 = G^{\gamma,\varepsilon}(W1, A1)$$

$$M2 = G^{\gamma,\varepsilon}(W2, A2)$$

The refined weight maps alongside the approximation and detailed coefficients will be given to the weighted fusion. By weighted fusion computation using refined weight maps A1 and A2 are merged to get the approximation coefficients as an and three point by point H1 and H2, V1 and V2, D1 and D2 to get wavelet coefficients. Finally the weighted fusion will give us the intertwined estimate and melded definite coefficients.

$$A = A1 \times M1 + A2 \times M2$$

$$H = H1 \times M1 + H2 \times M2$$

$$V = V1 \times M1 + V2 \times M2$$

$$D = D1 \times M1 + D2 \times M2$$

Inverse wavelet transform will be applied on the fused coefficients in order to get the original fused image.

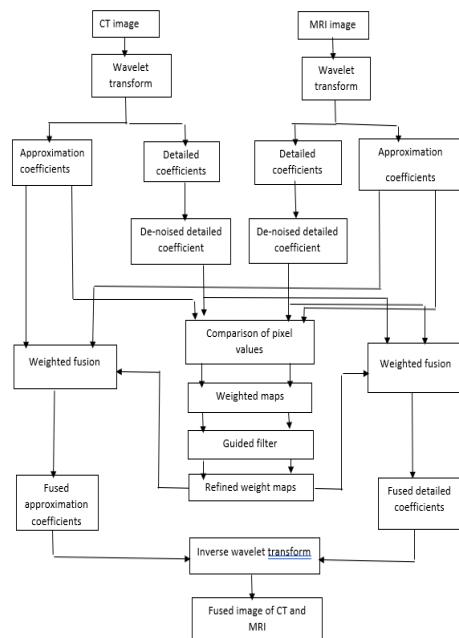


Fig : CT and MRI fusion of proposed algorithm

Stage 1: CT and MRI input image registration.

stage 2: In the way of applying wavelet transform CT image will give four coefficients as A1,H1,V1 and D1 comparably MRI picture will give four coefficients as A2,V2,D2 and H2. Also, the away from of CT and MRI images are denoised by utilizing a filter.

Stage 3: By taking a gander at the pixel estimations of approximation coefficients and wavelet coefficients of CT and MRI pictures, the weight maps are gotten and these weight maps filling in as the information picture, related approximation coefficients filling in as the guided image for the guided filter, if $A1 > A2$, $H1 > H2$, $V1 > V2$ and $D1 > D2$ then $W1=1$ in any case 0 equivalently if $A2 > A1$, $H2 > H1$, $V2 > V1$ and $D2 > D1$ then $W2=1$ in any case 0

$$W1 = \text{Max} (A1, H1, V1, D1)$$

$$W2 = \text{Max} (A2, H2, V2, D2)$$

Guided filter refine the weight maps and the resultant weight maps are called refined weight maps.

$$M1=G (W1, A1)$$

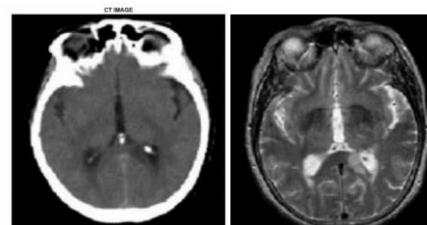
$$M2=G (W2, A2)$$

Stage 4 : Intertwined approximation and point by point coefficients can be gotten by utilizing weighted fusion algorithm.

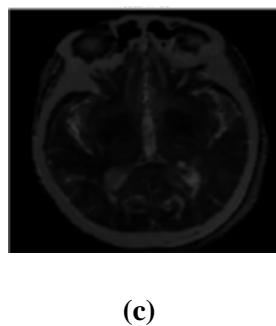
Stage 5: By applying inverse wavelet transform on approximation coefficients and detailed coefficients can be acquired.

V. EXPERIMENTAL RESULTS

The CT and MRI pictures of a comparable body segments will be taken as an input. Then we will get the combined picture as yield in the wake of applying wavelet change systems.



(a) (b)
Fig(a):CT (b) MRI image



(c)

Fig (c): Fused image by using haar wavelet transform

Table 1 : Evaluation of parameters of fused images of existing and proposed algorithms

Algorithm	Standard Deviation	Average Gradient
Choose-m	0.128938	0.188799
Fuzzy	0.129394	0.206837
Existing	0.150644	0.248909
Proposed	0.205963	0.259743

(Note: These are reference values)

CONCLUSION

Fundamentally in transform area, we utilize for the most part weighted coefficients for weighted fusion algorithm. Here in proposed GF structure, the weighted maps are filled in as input image and approximation coefficients are named as guided image. To get a refined weight map in the framework GF is utilized. These refined weight maps are remarkable in nature and utilizations fuzzy logic. Subsequently the proposed framework fuses the framework adaptively. By applying the wavelet transform on the CT and MRI images, approximation coefficients and 3 wavelet coefficients are gotten. The two approximation coefficients are contrasted with one another by pixel to pixel.

Presently to smooth the refined weight maps, GF is utilized. Here refined weight maps fuses the estimations of wavelet coefficients of CT and MRI images. Finally by utilizing reverse wavelet transform, intertwined CT and MRI images are acquired. Contrasted with different frameworks, the proposed framework gives the successful subtleties of CT and MRI pictures. Henceforth the proposed framework will improve the volume depiction in the framework. In future work GF is joined with multi-layer and multi-scale transform with the end goal of fusion algorithm.

REFERENCES :

1. Dual filter based image fusion algorithm for CT and MRI medical images .M.N.Narsaiah,S.Vathsal,
D.Venkat reddy.
2. Zhao, Y., Zhao, Q., Hao, A.: ‘Multimodal medical image fusion using improved multi-filter PCNN’, Biomed. Mater. Eng., 2014, 24, pp. 221–228
3. Chen, L., Pan, J., Chen, C.: ‘Clinical research of target contour in NPC IMRT using CT/MRI fusion technique’, Int. Med. Health Guid. News, 2008, 14, (1), pp. 4–7
3. Wang, L., Tao, L., Wang, H.: ‘The research on evaluate measure of CT and MRI image fusion’, J. Biomed. Eng. Res., 2006, 25, (4), pp. 247–250
4. Lizhen, C.A.O., Li, K., Zhao, X.: ‘The diagnostic application of registration of CT and MR images in craniocerebral tumour’, J. Clin. Radiol., 2004, 23, (12), pp. 1023–1026
5. Xing, Z., Lin, Z.: ‘Fusion of PET images with CT and MR images in diagnosing tumours’, Chin. J. CT MRI, 2005, 25, (5), p. 290
6. Wenqi, D., Yunfeng, Z., Yahua, Z.: ‘Application of CT and MRI image fusion in radiotherapy of head and neck tumours’, Chin. J. Radiat. Oncol. Biol., 2007, 16, (5), pp. 397–398
7. Rong, H., Hui, W., Xiaoxu, L.: ‘Observation of CT-MRI image fusion in post operative precise radiotherapy for gliomas’, Chin. J. Radiat. Oncol. Biol., 2017, 26, (2), pp. 192–196

8. Gan, X., Xu, Z., Liao, F.: ‘Application value of CT/MRI image fusion technique in the delineating of target area for radiotherapy of nasal pharyngeal cancer’, China Med. Dev., 2014, 29, (11), pp. 163–165
9. Xu, Q., Zhou, Y., Wang, W., et al.: ‘An algorithm of remote sensing image fusion based on nonsubsampled contourlet transform’. 2012 5th Int. Congress on Image and Signal Processing, Chongqing, China, 2012, pp. 1005–1009
10. Zhu, J., Che, J., Guo, Z.: ‘Curvelet algorithm of the remote sensing image fusion based on the local mean and standard deviation’, J. Ningxia Univ. (Nat. Sci. Ed.), 2014, 35, (1), pp. 24–27